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para-Sulfonatocalix[6]arene-modified silver nanoparticles electrodeposited on glassy carbon electrode: Preparation and electrochemical sensing of methyl parathion

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ABSTRACT

In this paper, a new electrochemical sensor, based on modified silver nanoparticles, was fabricated using one-step electrodeposition approach. The para-sulfonatocalix[6]arene-modified silver nanoparticles coated on glassy carbon electrode ($pSC₆$ -Ag NPs/GCE) was characterized by attenuated total reflection IR spectroscopy (ATR-IR), X-ray photoelectron spectroscopy (XPS) and scanning electron microscopy (SEM), etc. The pSC₆ as the host are highly efficient to capture organophosphates (OPs), which dramatically facilitates the enrichment of nitroaromatic OPs onto the electrochemical sensor surface. The combination of the host–guest supramolecular structure and the excellent electrochemical catalytic activities of the $pSC₆$ -Ag NPs/GCE provides a fast, simple, and sensitive electrochemical method for detecting nitroaromatic OPs. In this work, methyl parathion (MP) was used as a nitroaromatic OP model for testing the proposed sensor. In comparison with Ag NPs-modified electrode, the cathodic peak current of MP was amplified significantly. Differential pulse voltammetry was used for the simultaneous determination of MP. Under optimum conditions, the current increased linearly with the increasing concentration of MP in the range of 0.01–80 μ M, with a detection limit of 4.0 nM (S/N = 3). The fabrication reproducibility and stability of the sensor is better than that of enzyme-based electrodes. The possible underlying mechanism is discussed.

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1. Introduction

Organophosphates (OPs) are known to be highly neurotoxic and commonly used as chemical warfare agents and pesticides [\[1,2\]. A](#page-4-0)ll OPs irreversibly restrain the enzyme acetylcholinesterase (AChE), which is essential for the function of the central nervous system of humans and also of insects. The rapid detection of these toxic agents in the food, environment and public places has become increasingly important for homeland security and health protection. Analyzing OPs in environmental and food samples is routinely carried out using analytical techniques, such as gas liquid chromatography and mass spectrometry [\[3–7\].](#page-4-0) Although these methods are sensitive and accurate, they are generally performed at centralized laboratories, expensive instrumentation and often analysis results are not readily obtained, requiring quite some time to be available. The development of simple, cost effective, sensitive and selective analytical methods for fieldwork is of considerable interest.

Electrochemical sensors are simple, sensitive and selective devices for real-time monitoring of analytes of interest when properly designed. With the recent developments in nanotechnology, enzyme-based electrochemical biosensors towards OPs have been fabricated with nanoparticles enhancing electron transfer [\[8–15\].](#page-4-0) For instance, Lin and coworkers have reported a biosensor to detect OPs based on gold nanoparticles covalently coupled with acetylcholinesterase [\[16\]. L](#page-4-0)iu's group developed a sensitive OPs sensor composed of AChE antibody linked Zn at CdS NPs and $ZrO₂$ NPs which selectively captured phosphorylated acetylcholinesterase [\[17\]. T](#page-4-0)hough these enzyme-based devices usually allow high sensitivity due to the high loading of enzymes on the nanoparticles [\[18–21\], h](#page-5-0)owever, the stability of enzyme is limited since they tend to denaturation during immobilization and storage [\[22\]. T](#page-5-0)he artificial acceptors based on a host-molecule such as cyclodextrin, crown ether or calixarene, show good stability in solution and excellent binding ability towards organic molecules. para-Sulfonated calix[n]arene (pSC_n) [\[23\], a](#page-5-0) class of water-soluble calixarenes with open and rigid cavities, are interesting for molecular recognition. For instance, Barra and coworkers have showed that pSC_n can recognize phenol blue by the formation of host–guest complexes [\[24\].](#page-5-0)

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Scheme 1. Schematic diagram for one-step electrodeposition of pSC₆-Ag NPs on the surface of the GCE for MP sensing.

The ability of pSC_n to recognize various types of bisphenols was reported by Kitano and coworkers [\[25\]. T](#page-5-0)he pSC_n is a fine stabilizer and protective agent for metallic nanoparticles [\[26–28\]. T](#page-5-0)herefore, the fabrication of metallic NPs modified with pSC_n on the surface of electrode as electrochemical sensor is quite interesting.

In this work, the fabrication of a new pSC_6 modified Ag NPs electrochemically deposited on the surface of glassy carbon electrode (GCE) is reported aiming the electrochemical detection of nitroaromatic OPs. MP was used as a model (see Scheme 1). The detection of MP was performed rapidly with detection limit (DL) of 4.0 nM $(S/N = 3)$. The sensor opens a new opportunity for fast and sensitive determination of MP.

2. Experimental

2.1. Chemicals

Methyl parathion (MP) was provided by the Key Laboratory of Pesticide and Chemical Biology (CCNU), Ministry of Education, China. para-Sulfonatocalix[6]arene ($pSC₆$) was synthesized in the laboratory following procedure indicated as supporting information. Phosphate buffer solution (PBS) and other reagents were of analytical reagent grade. Aqueous solutions were prepared with doubly distilled water.

2.2. Instruments

Electrochemical measurements were performed on CHI-660C workstation (Shanghai, China) with a conventional three-electrode system with platinum wire as auxiliary electrode, saturated calomel electrode (SCE) as reference, and pSC_6 -Ag NPs modified glass carbon electrode (pSC_6 -Ag NPs/GCE) as working electrode. Scanning electron microscopy (SEM) was recorded by a Hitachi S-4700 electron microscope. X-ray photoelectron spectroscopy (XPS) was recorded by PHI Quantera SXM. Attenuated total reflection Fourier-transform infrared spectrum (ATR-FT-IR) was acquired with a Nexus 470 FT-IR (Nicolet, USA).

2.3. Preparation of $pSC₆$ -Ag NPs modified GCE

A GCE was polished with 0.3 and 0.05 μ m alumina slurry, then it was washed in a ultrasonic bath first with nitric acid solution (1:1, v/v), then with ethanol and finally with water (3 min each). The GCE was dried at room temperature.

A 0.1 M KNO₃ aqueous solution containing 0.2 mM AgNO₃ and 0.1 mM pSC_6 was used for electrodeposition of pSC_6 -Ag NPs at GCE electrodes. pSC_6 -Ag NPs were electrodeposited upon GCE electrodes by potential-sweeping electrodeposition. Electrodeposition was performed on a CHI 660 C electrochemical workstation (CH Instruments Inc.) with a conventional three-electrode system comprised of a platinum wire electrode, a SCE reference electrode, and GCE as the working electrode. The pSC_6 -Ag NPs can be formed on the GCE electrodes by cycling the potential of the working electrode between +0.40 and −0.10 V for a fixed time (for example, 110 s) [\[29,30\]. T](#page-5-0)hen the pSC_6 -Ag NPs/GCE was dipped into stirred water for 10 min to wash the excess $Ag⁺$ adsorbed on the surface of the electrode. The deposited electrode was dried in air at room temperature for about 3 h. The Ag NPs/GCE was prepared under the same conditions.

2.4. Electrochemical measurement of MP

The PBS buffer (pH 7.4) solution, used as the supporting electrolyte and the mixed solution was purged oxygen with pure nitrogen for 10 min after addition of MP solution. The modified electrode was immersed into the electrolyte, under stirring, and the accumulation of analyte was performed during 300 s at open circuit. Differential pulse voltammograms of the modified electrode were recorded between +0.15 and −0.90 V. The cathodic peak current was measured at −0.66 V. Cyclic voltammetry was performed under similar conditions.

2.5. Preparation of samples

The pear commercially available was used. A HR1861, PHILIPS blender was used to comminute and homogenize the fruit samples. After filtration, the fruit juice was spiked with 5 and 60 μ M of MP. For validation, fortified juice samples were analyzed after 1/100 dilution with water [\[3\].](#page-4-0)

Fig. 1. SEM images of (a) Ag NPs/GCE and (b) pSC_6 -Ag NPs/GCE when the electrode was magnified 85,000×, and both the bars are 100 nm.

3. Results and discussion

3.1. Optimization of the electrodeposition conditions and accumulation time

Three factors were considered when the electrodeposition conditions were optimized: (1) the mole ratio of pSC_6 and Ag^+ (n_{pSC6}/n_{Ag+}) , (2) the concentration of Ag⁺ (C_{Ag+}), and (3) the electrodeposition time. The cathodic peak current of MP reached the maximum when $n_{pSC6}/n_{\rm Ag+}$, C $_{\rm Ag+}$, and electrodeposition time were 1:2 ([Fig. S1\(a\)\)](#page-4-0), 2×10^{-4} M ([Fig. S1\(b\)\)](#page-4-0), and 110s [\(Fig. S1\(c\)\)](#page-4-0), respectively. Therefore, these conditions were used for further experiments.

The accumulation time for MP was studied ([Fig. S2\)](#page-4-0) and the maximum MP cathodic current was achieved using 300 s accumulation time. Three hundred seconds of accumulation time was thus employed in this work.

3.2. Characterization of $pSC₆$ -Ag NPs/GCE electrode

The XPS survey spectrum was measured to investigate the surface of modified electrode as shown in [Fig. S3. T](#page-4-0)he peak at 368 and 374 eV was assigned to Ag⁰ 3d_{5/2} and Ag⁰ 3d_{3/2}, which demonstrated that metallic Ag^{0} was formed on the surface of GCE by electrodeposition process. Fig. 1 shows the SEM images of Ag NPs and pSC_6 -Ag NPs formed on the surface of GCE by electrodeposition process, respectively. Compared with SEM image of Ag NPs on the surface of GCE (Fig. 1(a)), more pSC_6 -Ag NPs were observed in Fig. 1(b). It is reasonable to believe that $Ag⁺$ ions complexed with $pSC₆$ facilitating the reduction of Ag⁺ to form Ag NPs on the surface of electrode.

Fig. 2(b) and (c) shows the ATR-IR spectra of pSC_6 -Ag NPs and Ag NPs electrodeposited on GCE. Compared with the FT-IR spectrum of pure pSC_6 in Fig. 2(a), significant features can be seen in that of pSC₆-Ag NPs electrodeposited on GCE: the peaks for SO₃[–] at 1180 and 1116 cm⁻¹ found in pure pSC_6 , are shifted to 1166 and 1115 cm $^{\rm -1}$, respectively, which suggests that the SO $_3^-$ groups coordinate with the silver atoms on the surface of the Ag NPs. The dramatic differences among the data, especially of SO $_3$ [–], indicated that the $pSC₆$ was modified on the surface of Ag NPs. Compared with the ATR-IR spectrum of Ag NPs on GCE (Fig. $2(c)$), new peaks for SO₃[−] at 1166 and 1115 cm^{−1} appeared in Fig. 2(b) indicates the formation of pSC_6 -Ag NPs, and the peak at 1383 cm⁻¹ was assigned to the β (O–H) of pSC₆. Similar modification with parasulfonatocalix[6]arene on the surface of silver nanoparticles was shown in our previous work [\[26–28\]. T](#page-5-0)hese results demonstrated that the pSC_6 -Ag NPs were formed on the surface of GCE.

By using the Fe(CN) $_6^{3-/4-}$ redox pair as the electrochemical probe, the Nyquist plots of different electrodes in the frequency ranging from 0.01 to 100,000 Hz were obtained (Fig. 3). The redox

Fig. 2. FT-IR spectrum of (a) pSC_6 and ATR-IR spectra of (b) pSC_6 -Ag NPs and (c) Ag NPs deposited on the surface of GCE.

Fig. 3. (A) Electrochemical impedance spectroscopy of bare GCE (a), Ag/GCE (b) and pSC_6 -Ag NPs/GCE (c) in the electrolyte containing 5.0 mM Fe(CN) $_6^{4-/3-}$ and 0.1 M $KNO₃$. Inset is the equivalent circuit model used to fit the impedance data.

Fig. 4. Differential pulse voltammograms of 1 [×] ¹⁰−⁵ M MP at the Ag NPs/GCE (a); pSC_6 -Ag NPs/GCE (b). Inset: the current response of Ag NPs/GCE (a); pSC_6 -AgNPs/GCE (b) to MP. Supporting electrolyte, 0.01 M PBS (pH 7.4); scan rate, 100 mV s−1; accumulation time, 300 s.

process of the probe showed electron transfer resistance of about 390 Ω (curve a), 310 Ω (curve b), 900 Ω (curve c) at bare GCE, Ag/GCE and pSC_6 -Ag NPs/GCE, respectively. It suggested that Ag NPs on the surface of GCE improved the electron transfer, and organic $pSC₆$ blocked the electron transfer which was the indirect evidence of pSC_6 -Ag NPs deposited on the surface of electrode.

3.3. The high sensitivity of electrochemical detection MP

The well-defined cathodic peaks (P1c) at $-0.70V$ corresponding to the irreversible reduction of $-NO₂$ to hydroxylamine group ([Fig. S4,](#page-4-0) reaction 1) [\[29\]](#page-5-0) were observed in [Fig. S5.](#page-4-0) As shown in Fig. 4, the peak current (I_{p1c}) of MP measured by DPV at pSC_6 -Ag NPs/GCE was increased significantly by 20 times compared with that obtained at the Ag NPs/GCE, which suggested that pSC_6 -Ag NPs/GCE displayed excellent electrochemical catalytic activities towards MP. The possible reason is as follows: hydroxylamine (–NHOH), the reduction product of MP is partly protonated in neutral media. Thus, pSC_6 with the electron-rich cyclic cavity and the negative SO₃ $^-$ group can bind the aromatic and hydroxylamine of MP through host–guest interaction such as electrostatic interactions, cation– π interactions and π – π interactions [\[27\]. A](#page-5-0)nd the reduction of MP may be easier in electron-rich cyclic cavity of pSC_6 . For these reasons, the pSC_6 as an artificial acceptor can bind MP via host–guest interaction and catalyze the redox of MP, simultaneously.

3.4. Stability of pSC_6 -Ag NPs/GCE

In order to test the stability of the $pSC₆$ -Ag NP/GCE, it was submitted to rigorous conditions such as strong base solution (pH 14), strong acid solution (pH 1) and boiling water ($t = 100 °C$). As shown in Fig. 5, the pretreated pSC_6 -Ag NPs/GCE still displayed quite good electrochemical catalytic activities towards MP, although the current intensity is decreased by about 15% and 30% for acid solution and boiling water, respectively. Generally, the enzyme would lose bioactivity under those rigorous conditions. Therefore, the stability of pSC_6 -Ag NPs/GCE is better than that of enzyme modified electrodes.

Fig. 5. Differential pulse voltammograms of 1×10^{-5} M MP at the pSC₆-Ag NPs/GCE with pretreatment in strong base (pH 14), strong acid (pH 1), boiling water ($t = 100$ °C) for 10 min and without pretreatment. Supporting electrolyte, 0.01 M PBS (pH 7.4); scan rate, 100 mV s^{-1} ; accumulation time, 300 s.

3.5. Analytical performance

Fig. 6 displays the DPV response of MP by pSC_6 -Ag NPs/GCE. The cathodic peak currents (I_{p1c}) increase with the concentration of MP increasing. A linear relationship (R^2 = 0.997) between the current and the MP concentration was obtained in the range of 0.01–80 μ M. The linear regression equation is $I_p(\mu A) = 0.76 + 1.16 \times 10^{-5}$ C. The detection limit (DL) of the sensor was 4 nM (S/N = 3). Though the DL of this work is higher than the DLs (0.1 nM [\[30\],](#page-5-0) 0.4 pM [\[3\]\)](#page-4-0) of the reported OPs electrochemical sensors employing acetylcholinesterase, the stability of pSC_6 -Ag NPs/GCE is much better than that of enzyme modified electrodes, and the liner range is wider than some enzyme sensors [\(Table S1\).](#page-4-0)

When the concentration of MP was controlled at 1.0×10^{-5} M, good reproducibility was obtained with relative standard deviation (R.S.D.) of 4.28% for six parallel detections with the same

Fig. 6. Differential pulse voltammograms for MP at the pSC₆-Ag NPs/GCE. MP concentration (a–l): 1×10^{-8} , 5×10^{-8} , 1×10^{-7} , 5×10^{-7} , 1×10^{-6} , 5×10^{-6} , 1×10^{-5} , 2×10^{-5} , 4×10^{-5} , 5×10^{-5} , 6×10^{-5} , 8×10^{-5} M. Inset shows the calibration curve. Supporting electrolyte, 0.01 M PBS (pH 7.4); scan rate, 100 mV s−1; accumulation time, 300 s.

Fig. 7. The cathodic peak current response of pSC₆-Ag NPs/GCE in solutions containing 1 × 10⁻⁵ M MP in the absence and presence of 100-fold of PO₄^{3–} (a), SO₄^{2–} (b), CO_3^2 ⁻ (c), NO₃⁻ (d), 1 × 10⁻⁵ M *p*-nitrophenol (e) and nitrobenzene (f), respectively. Supporting electrolyte, 0.01 M PBS (pH 7.4); scan rate, 100 mV s⁻¹, accumulation time, 300 s.

modified electrode. Similarly, the fabrication reproducibility was estimated by using six different electrodes. A solution containing 1.0×10^{-5} M MP was determined by six electrodes, with a relative standard deviation of 3.6%, which indicated that the reproducibility of the electrode was excellent. The electrode retained a response of 98% of the initial current was retained for the electrode after it was stored in PBS (pH 7.4) at 7 ◦C for 10 days. After a 30 day storage period, the sensor retained 95% of its initial current response, and it showed no obvious decline after being used for 30 times.

Interferences arising from the other electroactive nitrophenyl derivatives and oxygen-containing inorganic ions (PO $_4{}^{3-}$, SO $_4{}^{2-}$, $CO₃^{2−}$, NO₃[−]) were used to evaluate the selectivity of the $pSC₆$ -Ag NPs/GCE to MP. Interfering experiments were performed with 1×10^{-5} M MP in the absence and presence of 1×10^{-5} M pnitrophenol, 1 × 10^{−5} M nitrobenzene, 100-fold of PO₄^{3−}, SO₄^{2−}, CO $_3{}^{2-}$ and NO $_3{}^-$. Fig. 7 shows the current signals of MP at different experimental conditions. PO $_4{}^{3-}$, SO $_4{}^{2-}$, CO $_3{}^{2-}$, NO $_3{}^-$ did not interfere the determination of MP with the peak current varies slightly, and p-nitrophenol, nitrobenzene produced scarcely any interferences though the reduction potentials of electroactive nitrophenyl derivatives are adjacent which could be partitioned. When the concentration of PO₄^{3–}, SO₄^{2–}, CO₃^{2–} and NO₃[–] were 1000-fold of MP, these inorganic ions did not interfere the determination of MP (Fig. S7A). And as shown in Fig. S7, when the concentration of p-nitrophenol, nitrobenzene was 10-fold of MP, p-nitrophenol produced scarcely any interference, but nitrobenzene produced obviously interference, and there were obviously interferences when the concentration of *p*-nitrophenol, nitrobenzene was 10fold of MP. These indicated that the pSC_6 -Ag NPs/GCE has potential application in the rapid determination of MP.

The concentration values of MP in the samples were determined by the proposed method. No voltammetric response corresponding to MP was observed when the real pear samples were analyzed, thus different quality of MP was added to the samples of 0.01 M PBS (pH 7.4), respectively. Standard-additions method was adopted to estimate the accuracy [\[31,32\]. T](#page-5-0)he results were summarized in Table 1. The recoveries were from 98.0% to 102.1%. These results demonstrated that it was a promising approach with high accuracy, precision and reproducibility. It can be used for the direct analysis of real relevant samples.

Recovery tests of MP in pear samples ($n = 5$).

4. Conclusions

The convenient and sensitive electrochemical sensor of pSC_6 -Ag NPs/GCE opens new opportunities for the analysis of MP. The process of fabrication the modified GCE was simple and convenient, the pSC_6 -Ag NPs electrodeposited on the GCE in one-step saved much more time compared with the surface of electrode modified through self-assembled monolayer (SAM). The specific complexation of MP on the surface of homemade pSC_6 -Ag NPs/GCE showed better stability than enzyme sensor which provides an effective quantitative method for MP analysis, and in comparison with Ag NPs-modified electrode, the cathodic peak current of MP was amplified significantly. The application of the sensor for determination of MP in the samples demonstrates that it is a promising and practical approach for the analysis of MP. Further variation of the sensor system could be achieved by modifying the Ag NPs with pSC_4 or pSC_8 , thus enabling the design of sensors for other substrates.

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Appendix A. Supplementary data

Supplementary data associated with this article can be found, in the online version, at doi:10.1016/j.talanta.2010.01.054.

References

- [1] B.A. Du, Z.P. Li, C.H. Liu, Angew. Chem. Int. Ed. 45 (2006) 8022–8055.
- [2] B.A. Gorman, P.S. Francis, D.E. Dunstan, N.W. Barnett, Chem. Commun. (2007) 395–397.
- [3] Q. Xiao, B. Hu, C.H. Yu, L.B. Xia, Z.C. Jiang, Talanta 69 (2006) 848–855.
- [4] S. Lacorte, D. Barcelo, Anal. Chem. 68 (1996) 2464–2471.
- [5] F. Hernandez, J.V. Sancho, O.J. Pozo, J. Anal. Bioanal. Chem. 382 (2005) 934–946.
- [6] N. Fidalgo-Used, M. Montes-Bayon, E. Blanco-Gonzalez, A. Sanz-Medel, Talanta 75 (2008) 710–716.
- [7] S. Lacorte, D. Barcelo, Envrion. Sci. Technol. 28 (1994) 1159–1163.
- [8] M.J. Banholzer, J.E. Millstone, L. Qin, C.A. Mirkin, Chem. Soc. Rev. 37 (2008)
- 885–897. [9] C.N. Lok, C.M. Ho, R. Chen, Q.Y. He, W.Y. Yu, H. Sun, P.K.H. Tam, J.F. Chiu, C.M.
- Che, J. Biol. Inorg. Chem. 12 (2007) 527–534.
- [10] H.D. Hill, R.A. Vega, C.A. Mirkin, Anal. Chem. 79 (2007) 9218–9223.
- [11] P. Zhou, Z. Dai, M. Fang, X. Huang, J. Bao, J. Phys. Chem. C 111 (2007) 12609–12616.
	- [12] S.Q. Liu, J.H. Yu, H.X. Ju, J. Electroanal. Chem. 540 (2003) 61–67.
- [13] Y. Xiao, H.X. Jun, H.Y. Chen, Anal. Chim. Acta 391 (1999) 73–82.
- [14] X. Yu, D. Chattopadhyay, I. Geleska, F. Papadimitrakopoulos, J.F. Ruslinng, Electrochem. Commun. 5 (2003) 408–411.
- [15] E. Topoglidis, A.E.G. Cass, B. O'Regan, J.R. Durant, J. Electroanal. Chem. 517 (2001) 20–27.
- [16] T.J. Lin, K.T. Huang, C.Y. Liu, Biosens. Bioelectron. 22 (2006) 513–518.
- [17] G.D. Liu, J.Wang, R. Barry, C. Petersen, C. Timchalk, P.L. Gassman, Y.H. Lin, Chem. Eur. J. 14 (2008) 9951–9959.
- [18] R.E. Ionescu, C. Gondran, L.A. Gheber, S. Cosnier, R.S. Marks, Anal. Chem. 76 (2004) 6808–6813.
- [19] G.D. Liu, Y.H. Lin, V. Ostatna, J. Wang, Chem. Commun. (2005) 3481–3483.
- [20] D. Shan, S. Cosnier, C. Mousty, Biosens. Bioelectron. 20 (2004) 390–396.
- [21] D. Shan, M.J. Zhu, E. Han, H.G. Xue, S. Cosnier, Biosens. Bioelectron. 23 (2007) 648–654.
- [22] E. Shoji, M.S. Freund, J. Am. Chem. Soc. 123 (2001) 3383–3384.
- [23] S. Shinkai, S. Mori, T. Tsubaki, T. Sone, O. Manabe, Tetrahedron Lett. 25 (1984) 5315–5318.
- [24] W.L. Tao, M. Barra, J. Org. Chem. 66 (2001) 2158–2160.
- [25] T. Nakaji-Hirabayashi, H. Endo, H.K.M. Gemmei-Ide, H. Kitano, Environ. Sci. Technol. 39 (2005) 5414–5420.
- [26] D.J. Xiong, M.L. Chen, H.B. Li, Chem. Commun. (2008) 880–882.

mann, Biosens. Bioelectron. 17 (2002) 1095–1105.

- [27] D.J. Xiong, H.B. Li, Nanotechnology 19 (2008) 465502–465507.
- [28] C.P. Han, L.L. Zeng, H.B. Li, G.Y. Xie, Sens. Actuators B 137 (2009) 704–709.
- [29] M.C. Tsai, P.Y. Chen, Talanta 76 (2008) 533–539;
- S. Marx, A. Zaltsman, I. Turyan, D. Mandler, Anal. Chem. 76 (2004) 120–126. [30] L. Shang, Y.L. Wang, L.J. Huang, S.J. Dong, Langmuir 23 (2007) 7738–7744.
- [31] G. Valdés-Ramírez, D. Fournier, M.T. Ramírez-Silva, J.-L. Marty, Talanta 74
- (2008) 741–746. [32] H. Schulze, E. Scherbaumb, M. Anastassiades, S. Vorlova, R.D. Schmid, T.T. Bach-